Application of a transition metal oxide/carbon-based nanocomposite for designing a molecularly imprinted poly (L-cysteine) electrochemical sensor for curcumin

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ABSTRACT

In this study an electrochemical sensor was fabricated for detection of curcumin, as a functional herbal food, using molecularly imprinted polymer and highly conductive transition metal oxide/carbon-based nanocomposite. In this way, CuCo2O4/nitrogen-doped carbon nanotubes/phosphorus-doped graphene oxide nanocomposite was dropped on the electrode. This nanocomposite synergically possesses conductivity features of copper and phosphorus-doping sites, specific surface area of carbon nanotubes, and carbons Fermi level of graphene oxide. In the following, L-Cystein electropolymerized on the electrode in presence of curcumin. The sensor was produced by removing curcumin from poly (L-cystein) matrix. The sensor was successfully used for detection of curcumin in the ranges of 0.1–1 µmol L–1 and 1–30 µmol L–1, with acceptable detection limit (30 nmol L–1). Finally, the proposed method was used for detection of curcumin in serum samples with recoveries of 80–110.87%. The results demonstrated that aforementioned method can be used for detection of curcumin in biological samples.

1. Introduction

Curcumin (CUR), as a diketone, 1,7-bis-(4-hydroxy-3-methoxy-phenyl)-1,6-heptadiene- 2,5-dione, can be extracted from turmeric rhizome which belongs to the ginger family. CUR has been widely used with dietary and therapeutic aims. This compound, as natural pigment with bright yellow color, can be applied in industrial dyeing consumptions such as production of cakes, canned foods, and beverages. Also due to functional effects of anti-oxidizing, anti-bacterial, anti- carcinogenicity, anti-inflammatory, and anti-HIV, this compound is considered as a potent herbal agent in biology and pharmacology (Neerati, Devde, & Gangi, 2014). So, because of growing use of CUR as a functional herbal food, the development of the analytical method for its quantification in biological and food samples is highly demanded.

Up to now several analytical methods have been developed for detection of CUR such as liquid chromatography, capillary electrophoresis (CE), spectrophotometry, resonance light scattering (RLS) and spectrofluorimetry (Liu, Gong, Dong, Zhou, Shuang, & Dong, 2018). Although these methods may possess high enough sensitivity and accuracy, but they suffer from requirement of costly equipment and reagents, boring and complex sample preparation, lack of selectivity and expert persons. In comparison with aforementioned methods, electrochemical sensors are highly simple, sensitive and facile which can be a powerful alternative of traditional methods for CUR detection.

Abbreviations: CUR, Curcumin; MIP, Molecularly imprinted polymer; P-GO, Phosphorous-doped graphene oxide; N-CNTs, Nitrogen-doped carbon nanotubes; L-Cys, l-cysteine.

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Recently modification of electrochemical sensors with metal nanoparticles, and carbon nanomaterials has gained considerable attention. Carbon nanotubes (CNTs) with significant conductivity and high surface area are a potent modifier agent for electrochemical sensors. Moreover, doping of nitrogen can lead to the enhancement of conductivity and stability of CNTs (Zhang, Sui, Xue, Wang, Pei, Liang, et al., 2019).

CuCo$_2$O$_4$ nanomaterials, as oxides of transition metal, possess unbelievable properties such as stability, catalytic effects, simple and low-cost synthesis, specific surface area and conductivity. So, incorporation of CuCo$_2$O$_4$ nanomaterials with CNTs can devote excellent electrochemical features to sensors.

Graphene as 2D carbon material contain packed carbon atoms in unit sheet of hexagonal structure. Graphene with interesting physical, electrical and optical features, have been an attractive material for fabrication of sensors. The possible irreversible agglomeration of graphene nanosheets due to $\pi$-$\pi$ and Van-der-Waals interactions may limit its application. Collaboration of 1D CNTs with graphene can improve efficiency of graphene through playing role of electron transfer between sheets and prevention of agglomeration. On the other hand, chemical doping of graphene by heteroatoms such as sulfur, nitrogen, phosphorus, and boron can lead to prevention of aggregation and enhancement of conductivity (Xu, Liu, Chen, Li, Tang, & Li, 2017).

Molecularly imprinted polymers (MIP) as a cross-linked polymer are commonly formed through electrochemically polymerization of functional monomers and template on the sensors. MIP contains recognition sites formed by interaction between template and monomer followed by extraction and removal of template. So, MIP can improve the specifically recognition ability of sensors to template.

In this study, glassy carbon electrode (GCE) was modified by CuCo$_2$O$_4$/nitrogen-doped CNTs/phosphorous-doped graphene oxide nanocomposite (CuCo$_2$O$_4$/N-CNTs/P-GO) followed by electropolymerization of l-cysteine (l-Cys), as functional monomer, in presence of CUR (Scheme 1). l-Cys as an important amino acid is able to be applied for electropolymerization due to the electro activity of amino and thiol groups. Based on our knowledge, the application of CuCo$_2$O$_4$/N-CNTs/P-GO nanocomposite and incorporation of CuCo$_2$O$_4$/N-CNTs/P-GO with MIP for the first time have been performed for designing a sensor for CUR detection. Finally, the designed electrode was successfully used for detection of CUR in serum sample.

2. Material and methods

2.1. Chemicals

Copper (II) acetate monohydrate (Cu(OAc)$_2$$\cdot$H$_2$O), Cobalt (II) acetate tetrahydrate (Co(OAc)$_2$$\cdot$4H$_2$O), CUR, potassium ferricyanide (K$_3$[Fe(CN)$_6$)$_2$), monobasic sodium phosphate (NaH$_2$PO$_4$), dibasic sodium phosphate (Na$_2$HPO$_4$), phosphoric acid (85%, analytical grade), graphite flakes (grade 230U, 325 mesh), polyphosphoric acid (105% H$_3$PO$_4$ basis), multi-walled carbon nanotubes (MWCNTs), l-Cys, potassium permanganate (KMnO$_4$), potassium nitrate (KNO$_3$), were all obtained from Sigma-Aldrich (USA). All solvents with analytical grade such as ethanol, sulphuric acid (H$_2$SO$_4$), hydrochloric acid (HCl), ammonia solution (NH$_3$$\cdot$H$_2$O) and hydrogen peroxide (H$_2$O$_2$) were...
purchased from Merck (USA). The stock solution of CUR was prepared by ethanol and was kept in dark and 4°C until use.

2.2. Instruments

All electrochemical detection processes were performed using Autolab potentiostat–galvanostat three-electrode system (PGSTAT204, Metrohm, Herisau, Switzerland) containing Ag/AgCl reference electrode, platinum counter electrode and GCE as working electrode. The studies of electrochemical impedance spectroscopy (EIS) were performed by Autolab 302 N system. Analysis of data was done by NOVA 1.11 software. A LEO 912AB (120 kv, Germany) system was used to obtain transmission electron microscopy (TEM) image. X-ray spectroscopy (EDX) image, surface morphology and elemental MAPING were obtained by a MIRA3 TESCAN (USA) Field Emission Scanning Electron Microscope (FE-SEM) with LVSTD detector (USA). Energy-dispersive X-ray diffraction (XRD) spectra was recorded by an Explorer system (GNR Co., Italy) equipped with a radiation source of Cu Kα (1.54187 Å) and Scintillator detector working at conditions of 30 mA, 40 kV and room temperature. A NanoWizard II system (JPKCo., Germany) was used for preparing atomic force microscopy (AFM) images. Fourier transform infrared (FTIR) spectra were achieved by Thermo Nicolet spectrophotometer (made in USA, model of AVATAR 370). The studies of X-ray photoelectron spectroscopy (XPS) for obtaining the binding energies of nanoparticles were done by PHI Quantera II Scanning XPS Microprobe equipped with a Al Ka anode as monochromatic radiation source under conditions of 1486.6 eV, pressure < 2 × 10⁻⁶ bar and room temperature.

2.3. Synthesis of CuCo₂O₄/N-CNTs

Preparation of CuCo₂O₄/N-CNTs was done according to the previous studies with some modifications (P. Liang, Wang, & Hu, 2018). Firstly, for oxidation, 100 mg MWCNTs were added to 23 mL sulfuric acid followed by stirring for 12 h. After sequentially addition of 416 mg KNO₃ and 1 g KMnO₄ to the mixture in a 40°C water bath, 6 mL water was sectionally added with an interval time of 5 min. Then after another 5 min, 15 mL water was added and the mixture stayed unchanged for 15 min. Afterwards 10 mL H₂O₂ (30%) and 140 mL water were added to complete the oxidation reaction. The resultant was collected and washed with water and HCl (5%) solution. Afterwards, 0.086 g of oxidized CNTs sonicated in 4 mL of water–ethanol composition (4:96, v/v %). After addition of 0.128 g Cu(OAc)₂⋅H₂O and 0.31 g Co(OAc)₂⋅4H₂O, 0.5 mL NH₃⋅H₂O was added and mixture was stirred for 24 h at 80°C. After addition of aforementioned mixture to the stainless-steel autoclave reactor, hydrothermal reaction was processed at 150°C for 1 h. After completion of reaction, the resultant was centrifuged, collected, washed with ethanol–water (50:50, v/v %) and freeze-dried.

2.4. Synthesis of P-GO

The protocol of synthesis was processed with orderly performance of three steps containing oxidation, exfoliation and phosphonation according to the previous reported studies (Abouzari-Lotf, Zakert, Nasef, Miyake, Mozarrinia, Bazilah, et al., 2019). Firstly, GO was obtained by oxidation of graphite flakes according to the Hummers and Offeman method followed by exfoliation step which was performed by ultrasonication of resultant (4 mg mL⁻¹) in water. In order to removal of unexfoliated residual, the mixture was centrifuged for 15 min (1610 g,
10°C. Finally resulted GO powder was dried in a vacuum oven at 70°C for 24 h. For phosphonation process a mixture of polyphosphoric acid and phosphoric acid (1:5 wt%) homogenized by sonication and its pH was adjusted to 5 and then added into a flask. After dispersion of GO in 50 mL deionized water (DI) (0.5 wt%), the mixture was poured into the experimental flask followed by stirring and heating (95°C) for 8 h. Finally, the resultant centrifuged (12175 g, 2°C), washed by DI and dried in the vacuum condition.

2.6. Pretreatment of human serum samples

The blood serum sample was obtained from a local clinical pathology laboratory and used without pretreatment. According to the previous study, the serum sample was prepared by 100 times dilution (Kalambate, Rawool, & Srivastava, 2016) by PBS (pH 3.06, 0.1 mol L⁻¹).

3. Results and discussion

3.1. Preparation and characterization of the sensor

In order to the detection of CUR, in a volumetric flask a proper volume of CUR stock solution diluted by PBS (pH 3.06, 0.1 mol L⁻¹) to 4 mL to obtain considered concentration followed by detection by differential pulse voltammetry (DPV) mode. Also, for application of detection method in real sample, prepared serum was spiked by proper volume of CUR stock solution.
figures for individual characterization of nanoparticles were considered as supplementary information. Fig S1 and Fig S2 presence characterization images related to CuCo2O4/N-CNTs and P-GO, respectively.

In order to ideal performance of electrode modification, both nanoparticles must be homogeneously mixed before dropping on the electrode surface. CUR can be adsorbed on the electrode surface through non-covalence interaction with nitrogen groups (Mousaabadi, Ensafi, Hadadzadeh, & Rezaei, 2020) and phosphonic acids groups for further polymerization process. The surface morphology of CuCo2O4/N-CNTs/ P-GO nanocomposite was evaluated by FE-SEM technique. As presented in Fig. 1A CuCo2O4/N-CNTs nanoparticles and P-GO nanosheets were uniformly and homogeneously mixed and CuCo2O4/N-CNTs nanoparticles were well distributed among P-GO nanosheets. Moreover, incorporation of CuCo2O4 nanoparticles with size about 100 nm on the N-CNTs was proved. In addition, elemental analysis of CuCo2O4/N-CNTs/ P-GO nanocomposite was done by EDX and MAPING analysis (Fig. S3).

CuCo2O4 as multivalent metal oxides possess spinal structure which copper ions locate on tetrahedral position and cobalt ions locate on both tetrahedron and octahedron position (Z.-H. Liang, Zhu, & Hu, 2004). So, the L-Cys can be anchored on the surface through binding of carboxyl, thiol and amino groups of L-Cys to cobalt and copper (Priyanga, Khamrang, Velusamy, Karthi, Ashokkumar, & Mayilmurugan, 2019; Zhou, Mo, Sun, Luo, Fan, Zhu, et al., 2022). Also, hydrogen bonding of L-Cys with phosphonic acids groups of P-GO lead to anchoring on the electrode surface. Especially according to the literature, anchoring of L-Cys on the carbon groups of nanoparticles can be happened through amino groups of L-Cys during electrochemical oxidation process followed by consecutive nucleophilic acyl substitution (He, Li, Zhang, & Luo, 2017). The incorporation of CUR in poly (L-Cys) matrix is through hydrogen bonding interactions with oxygen groups of CUR (Scheme 1).

Molecular imprinted poly (L-Cys) layer was created on the surface of GCE/CuCo2O4/N-CNTs/P-GO by electropolymerization of L-Cys during 20 cycles from 0.6 to 0.6 V with scan rate of 50 mV s^-1 in pH 7 PBS (0.05 mol L^-1) containing CUR and L-Cys (CUR: L-Cys mole ratio 1:2).

As shown in the cyclic voltammograms (Fig. 1B), when cycles consecutively scanned with scan rate of 50 mV s^-1 in the considered ranges, the oxidation and reduction peaks current of L-Cys at about 0.1 and 0.5 V were dramatically decreased which demonstrates successfully, preparation and growth of insulating polymer layer. Moreover, for removal of CUR from poly (L-Cys) and creation of specific cavities, 40 cycles were scanned (Fig. 1C) in PBS with pH 7 (0.05 mol L^-1) in the potential range of 0.6–0.6 V. According to the Fig. 1C the disappearance of anodic and cathodic peak currents at about 0.2 V during consecutive scans, obviously demonstrates the removal of CUR from poly (L-Cys) matrix. The CV results of preparation of proposed sensor are presented in Fig. 1D. The increase of current of GCE/CuCo2O4/N-CNTs/P-GO/CUR- incorporated poly (L-Cys) (Fig. 1D, curve a) in comparison with GCE (Fig. 1D, curve c) obviously demonstrated effect of coating the electrode by CuCo2O4/N-CNTs/P-GO nanocomposite and poly (L-Cys). Moreover elimination of anodic and cathodic peak currents at about 0.2 V for GCE/CuCo2O4/N-CNTs/P-GO/CUR-imprinted poly (L-Cys) (Fig. 1D, curve b) clearly proved successfully removal CUR from poly (L-Cys) matrix.

In order to more confirmation, FT-IR spectroscopy was applied for identification of GCE modification and results are indicated in the Fig. 2A. As shown in FT-IR spectrum of CuCo2O4/N-CNTs (Fig. 2A, curve a) the presence of –COOH groups are proven by vibration peaks.

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Fig. 3. Evaluation of surface modification by CV: (A) linear diagram of peak current of K3Fe(CN)6 (1 mmol L^-1) against square root of scan rate in the range of 10–100 mV s^-1; (B) (a-c) Cyclic voltammograms of K3Fe(CN)6 (1 mmol L^-1) scanned by (a) GCE, (b) GCE/ CuCo2O4/N-CNTs/ P-GO, and (c) GCE/CuCo2O4/N-CNTs/ P-GO/CUR- imprinted poly (L-Cys); (C) Cyclic voltammograms of K3Fe(CN)6 (1 mmol L^-1) at scan rate of 50 mV s^-1 obtained by: (a) GCE/CuCo2O4/N-CNTs/ P-GO/CUR- incorporated poly (L-Cys), (b) GCE/ CuCo2O4/N-CNTs/ P-GO, (c) GCE/CuCo2O4/N-CNTs/ P-GO/CUR- incorporated poly (L-Cys), (d) GCE. (A-C) condition: Start and stop potential: −0.6, Upper potential: 0.6, CUR to L-Cys mole ratio: 1:2, Electrolyte: KCl 100 mmol L^-1, (D) Nyquist plots obtained from 1 mmol L^-1 K3Fe(CN)6 (solvated in KCl 100 mmol L^-1) in the frequency range of 10^-2 to 10^5 Hz by: (a) GCE/CuCo2O4/N-CNTs/ P-GO/CUR- imprinted poly (L-Cys), (b) GCE/ CuCo2O4/N-CNTs/ P-GO, (c) GCE.
related to the O–H stretching (3367 cm$^{-1}$), O–H bending (563 cm$^{-1}$), C–O stretching (1393 cm$^{-1}$, 1125 cm$^{-1}$), and C=O (1650 cm$^{-1}$). Moreover the peaks appeared at 2400 cm$^{-1}$ (carbonitrile groups; RC≡N), 1415 cm$^{-1}$ (C=N in pyridinic groups), 1640 cm$^{-1}$ (C=C inCNTs), 1564 cm$^{-1}$ (C=N groups) and 653 cm$^{-1}$ (C=O in CuCo$_2$O$_4$) assigned to successful synthesis of CuCo$_2$O$_4$/N-CNTs. The P-GO FT-IR spectrum (Fig. 2A, curve b) shows stretching peaks of C–P, P=O, P–O, and P=O at 1128 cm$^{-1}$, 1167 cm$^{-1}$, 1058 cm$^{-1}$, and 932 cm$^{-1}$ respectively. Moreover, stretching peaks of P–H, C=–C, C=O are centered at 2406 cm$^{-1}$, 1604 cm$^{-1}$, 1723 cm$^{-1}$, respectively. The overlapping and broadening of stretching peak of OH with CH$_2$ at 2917 cm$^{-1}$ and 2846 cm$^{-1}$ demonstrating the formation of phosphonic acid groups and less containing of carbonylic acid on GO (Tsetasmi, Abouzari-Lotfi, Ripin, Nasef, Ting, Saharkhiz et al., 2018).

The successful formation of poly (L-Cys) on the surface of CuCo$_2$O$_4$/N-CNTs/P-GO was checked by FT-IR spectroscopy. As shown in the Fig. 2A, curve e the absorption peaks are appeared at 3438 cm$^{-1}$ is related to N–H stretching which is sharpened due to overlapping with O–H stretching band of CuCo$_2$O$_4$/N-CNTs at 3367 cm$^{-1}$. It worth to mention that electrochemical oxidation of i-Cys on the surface lead to creation of cysteic acid which can be confirmed by appearance of adsorption bands at 1631 cm$^{-1}$ as the combinational peak of stretching vibrations of C=O and C–N, and 1064 cm$^{-1}$ as stretching vibrations of C–N. Moreover absence of stretching vibration of S=O group of cysteic at 2550 cm$^{-1}$ (Fig. 2A, curve d) in comparison with poly (L-Cys) (Fig. 2A, curve c) proved oxidation of S=O to SO$_2$H (S. Jiang, Wang, Ding, & Luo, 2015). As presented in Fig. 2B, curve c (and Fig. 2A, curve c) the main vibration absorption bands of CUR are at 810 cm$^{-1}$ (C=H), 963 cm$^{-1}$ (aliphatic –C–O), 1281 cm$^{-1}$ (aromatic –C–O), 1510 cm$^{-1}$ (C=C), 1627 cm$^{-1}$ (C=O), and C–H (3341 cm$^{-1}$), which considerably covered by poly (L-Cys) (Fig. 2A, curve a, and Fig. 2B, curve b) which is in accordance with absorption bands presented in literature (Mars, Mejri, Hamzaoui, & Elfi, 2021). Also, as shown in Fig. 2B the FT-IR bands of poly (L-Cys)-CUR (Fig. 2B, curve b) possess stronger intensity and shift in comparison with poly (L-Cys) after removal of CUR (Fig. 2B, curve a), which obviously demonstrates that successful extraction procedure.

The further analysis of electrode morphology and topography was performed by AFM. According to the AFM images (Fig. 2C), nanoparticle uniformly covered electrode surface. As shown in Fig. 2C (part b) after formation of polymeric layer of poly (L-Cys)-CUR, the particles size increased in comparison with nanoparticles (Fig. 2C, part a). After removal of CUR from the polymeric layer, larger cavities (Fig. 2C, part c) were presented between particles demonstrating the successful formation of CUR-imprinted poly (L-Cys) on the electrode surface. Also, the root-mean-square (RMS) values, which used for expression of the surface roughness, obviously increased from 3.78 for nanoparticles to 5.56 nm for poly (L-Cys)-CUR demonstrating successful formation of polymeric layer. Also, RMS value increased to 29.47 nm for CUR-imprinted poly (L-Cys), which can be due to successful removal of CUR from poly (L-Cys) layer.

### 3.2. Cyclic voltammetry studies

In order to evaluation of effect of modifiers on the surface of the electrode, cyclic voltammograms were scanned in a solution of 1 mmol L$^{-1}$ K$_3$[Fe (CN)$_6$] and 0.1 mol L$^{-1}$ KCl to estimate the active surface area of electrodes using Randles-Sevcik equation (Eq. (1)) as follow (Motia, Bouchikhi, & El Bar, 2021):

$$I_p = 2.69 \times 10^5 n^{3/2} A D^{1/2} C a^{1/2}$$  \hspace{1cm} (1)

where $I_p$, n, A, D$_0$, n and C$_0$ and $a$ are related to the anodic peak current (amps), the number of electrons, the surface area of the electrode (cm$^2$), the diffusion coefficient (cm$^2$ s$^{-1}$), the number of electrons, the concentration (mol cm$^{-3}$) of K$_3$[Fe (CN)$_6$] in bulk solution and the scan rate (V s$^{-1}$), respectively. For redox aforementioned system (Fe (CN)$_6^{3-/4-}$) n and $D_0$ values are 1 and 7.6 $\times$ 10$^{-9}$ cm$^2$ s$^{-1}$, respectively (Motia, Bouchikhi, & El Bar, 2021). Randles-Sevcik equation is related to an electrochemical reaction depended to the electrode potential and diffusion (Zaith & Athar, 2015). According to the Fig. 3A, by increasing scan rate, the cathodic and anodic peaks gradually increased and also there are a good relationship (Fig. 3B) between peak currents and square root of scan rate demonstrating diffusion controlled by mass transport (Wang, Chen, Li, Zhou, Guo, Kang, et al., 2018). The process of electron transfer can be mass transport if the process is wholly diffusion (Zaith & Athar, 2015).

For calculation of surface area changes, the cyclic voltammograms of GCE (Fig. 3A, part a), GCE/CuCo$_2$O$_4$/N-CNTs/P-GO (Fig. 3A, part b) and GCE/CuCo$_2$O$_4$/N-CNTs/P-GO/CUR-imprinted poly (L-Cys) (Fig. 3A, part c) in a solution of 1 mmol L$^{-1}$ K$_3$[Fe (CN)$_6$] were scanned by increasing of scan rate from 10 mV s$^{-1}$ to 100 mV s$^{-1}$. Using results of Fig. 3A, the alterations of anodic peak current (peak height; $I_p$) versus $u^{1/2}$ were plotted (Fig. 3B), and active surface area of GCE, GCE/CuCo$_2$O$_4$/N-CNTs/P-GO and GCE/CuCo$_2$O$_4$/N-CNTs/P-GO/CUR-imprinted poly (L-Cys) were calculated 0.135 cm$^2$, 0.27 cm$^2$ and 0.54 cm$^2$, respectively, according to the Eq. (1). These indicates the improvement of surface area about 2 times with comparison of GCE and GCE/CuCo$_2$O$_4$/N-CNTs/P-GO, and 2 times with comparison of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO and GCE/CuCo$_2$O$_4$/N-CNTs/P-GO/CUR-imprinted poly (L-Cys). These phenomena proved effect of nanocomposite and creation of cavities on modification of electrode.

As shown in Fig. 3(C) redox peak current of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO (Fig. 3C, curve b) was enhanced compared with GCE (Fig. 3C, curve d) due to high electron transfer capability of nanocomposite. According to the literature, CuCo$_2$O$_4$ and N-CNTs are synergically able to enhancement conductivity and electrocatalytic activities due to increase of catalytic sites of Cu doping such as Cu$^{2+}$ and Cu–N on the high specific surface area of CNTs which served as substrate for CuCo$_2$O$_4$ (Cheng, Li, Su, Li, & Liu, 2017). Also, due to the electron-donor ability of P-doping and increase of conducting electrons density at Fermi level of carbon, the potential of electron transferring and conductivity of P-GO can be improved (X. Ma, Ning, Qi, Xu, & Gao, 2014).

The formation of poly (L-Cys)-CUR on the surface of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO, led to somewhat decrease of redox peak current (peak height) due to the electron transfer hindrance (Fig. 3C, curve c). After elution of CUR molecules from poly (L-Cys), the current response (Fig. 3C, curve a) was considerably increased due to elimination of electron transfer hindrance of CUR molecules and creation of CUR-imprinted cavities leading to the enhancement of rate of electron transfer. According to the Fig. 3(C) peak potential separation ($\Delta$Ep) of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO was 0.17 V which was significantly lower than $\Delta$Ep (0.27 V) of GCE demonstrating catalytic effect of the nanocomposite. Moreover, formation of CUR-imprinted poly (L-Cys) on the surface of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO decreased $\Delta$Ep (0.105 V) due to poly (L-Cys) conductivity and formation of a lot of cavities which facilitate electron transfer.

### 3.3. EIS analysis

The resistance of electrode in different steps of modification can be performed by EIS using Nyquist impedance spectrum containing the semicircular section at higher frequencies and the linear section at lower frequencies (Kor & Zarei, 2016). The later indicates the diffusion-limiting process and the former is related to electrode transfer resistance ($R_d$). In accordance with resulted Nyquist diagram, the possible circuit (Fig. 3D, inset) contained members including solution resistance ($R_s$), double layer capacitance ($C_d$), $R_w$, and Warburg impedance ($Z_w$) which was in series with $R_s$ and is related to the Nernstian diffusion. According to the fitted circuit, $R_s$ is the only key element which describe the electrode kinetics for charge transfer (Kor & Zarei, 2016). According to the Nyquist impedance spectrum (Fig. 3D) which was obtained in 1 mmol L$^{-1}$ K$_3$[Fe(CN)$_6$] solution, $R_s$, value of GCE/CuCo$_2$O$_4$/N-CNTs/P-GO
(249 Ω) (Fig. 3D, curve b) is lower than GCE (339 Ω) (Fig. 3D, curve c). This phenomenon can be due to high conductivity and surface to volume ratio of nanocomposition which led to increasing rate of electron transfer. Fig. 3D indicates formation of MIP considerably reduced $R_{ct}$ to 4 Ω (Fig. 3D, curve a) and the reduce of semicircle radius demonstrating successful removal of CUR from poly (l-Cys) matrix and formation of numerous cavities which promotes electron transfer pathways.

3.4. Determination of CUR

In order to quantification of CUR, DPV mode with was used due to advantages of peak sharpening, great sensitivity and low background. As shown in Scheme 1 after electropolymerization of l-Cys on the GCE/CuCo$_2$O$_4$/N-CNTs/P-GO by consecutive nucleophilic acyl substitution (He, Li, Zhang, & Luo, 2017), CUR trapped in poly (l-Cys) matrix through hydrogen bonding interactions. After removal of CUR, numerous selective cavities which were complementary in functional groups and shape with CUR were created. After rebinding of CUR, one electron oxidation process led to creation of DPV peak (Q. Zhou, Zhai, Pan, & Li, 2017). As shown in Fig. 4A and Fig. 4B oxidation peaks of CUR were increased by increase of CUR in range of 0.1–30 µmol L$^{-1}$. The resulted data of proposed sensor for detection of CUR was compared with previous studies. The summarized data of Table 1 obviously demonstrated that linear range and LOD of present study was acceptable in comparison with other studies and proposed sensor was successfully designed for detection of CUR. According to the information was reported in Table 1, although some chromatography-based studies possess better linear range or LOD, but these methods are highly depended on the complex and expensive equipment and highly experienced experts in comparison with electrochemical sensors. Moreover, other reported sensors for CUR have not been designed based on incorporation of nanoparticles with MIP which can donate sensitivity and selectivity to designed sensor.

Due to validation of method, different parameter such as repeatability, precision, bias and accuracy of proposed method for intra-day ($n = 4$) and inter-day ($n = 4$) detection of CUR were evaluated according to the previous study (Kalambate, Rawool, & Srivastava, 2016). Moreover, the recovery was estimated using calibration curve. According to the results of Table 2, acceptable precision and accuracy of proposed method for detection of CUR were confirmed.

3.5. Binding studies

In order to demonstration of imprinted polymers superiority, evaluation of binding constants is necessary. Due to the presence of numerous heterogeneous binding sites in non-covalently MIP,
proficiency of MIP for analytical procedure may be decreased and led to the cross-reactivity during binding assay (Schauperl & Lewis, 2015). So, recognition and estimation of the heterogeneity and different sites can be important. For this purpose, the binding isotherms is determined using detection responses related to a range of concentration. Subsequently a suitable model is fit to the binding isotherm to evaluate the binding parameters. The Langmuir isotherm is a prevalent model which have been used (Pesavento, Marchetti, De Maria, Zeni, & Cennamo, 2019).

According to the previous study (Pesavento, Marchetti, De Maria, Zeni, & Cennamo, 2019), binding evaluation of synthesized polymeric layer was performed using following equation (Eq. (2)) related to Langmuir model:

\[
S = \frac{k_C k_A [A]}{1 + k_A [A]}
\]  

(2)

The linearized form of Eq. (2) is as follow:

\[
S = \frac{K_a S + K_a k_C}{K_a}
\]  

(3)

The parameters of Eq. (2) and Eq. (3) such as \( S, [A], K_a, k, \) and \( q \) are known as signal, target concentration (mol L\(^{-1}\)), association constant (L mol\(^{-1}\)), transduction method constant, and sites concentration, respectively. As shown in Fig. 4D, the binding isotherm plot was curved at high concentrations due to saturation which is in accordance with Langmuir model. Moreover, curved Scatchard plot (Fig. 4E) indicated two straight lines related to the presence of two different kinds of sites with high and low affinity, due to the complete and incomplete interaction between CUR and poly (l-Cys) (Mohammadinejad, Kamran Rad, Karimi, Motamedshariaty, & Mohajeri, 2021). Also, according to the Eq. (3), values of \( K_a \) for high and low affinity binding sites were calculated 2.52 \( \times \) 10\(^{-4}\) L mol\(^{-1}\) and 3.03 \( \times \) 10\(^{-5}\) L mol\(^{-1}\), respectively. The selectivity and specificity of prepared imprinted polymer can be evaluated by \( K_a \) (Hasanah, Rahayu, Pratiwi, Rotinawati, Megantara, Saputri, et al., 2019). The estimated values of \( K_a \) were in acceptable range in comparison with \( K_a \) values reported by previous studies which introduced MIP-based sensors for ethyl carbamate (\( K_a 4.75 \times 10^9 \) L mol\(^{-1}\)) (Guo, Hu, Wang, Brodelius, & Sun, 2018)), erthyroycin (\( K_a 6.25 \times 10^6 \) L mol\(^{-1}\)) (Sari, Uzek, Duman, & Denizli, 2016)), dopamine (\( K_a 2.9 \times 10^4 \) L mol\(^{-1}\)) (Li, Zhang, Sun, Bai, & Zheng, 2016)), methyl parathion (\( K_a 0.029 \) L mg\(^{-1}\)) (Zokhtareh, Bagheri, & Rahimnejad, 2018)), fructose (\( K_a 4.1 \times 10^2 \) L mol\(^{-1}\)) (Nikitina, Zaryanov, Kochetkov, Karyakina, Yatsimirsky, & Karyakin, 2017)), lactate (\( K_a 1.50 \times 10^2 \) L mol\(^{-1}\)) (Nikitina, Zaryanov, Kochetkov, Karyakina, Yatsimirsky, & Karyakin, 2017)), and glucose

<table>
<thead>
<tr>
<th>Sensor/Extraction method</th>
<th>Detection</th>
<th>Linear range</th>
<th>LOD</th>
<th>Sample</th>
<th>Recovery</th>
<th>Reference</th>
</tr>
</thead>
<tbody>
<tr>
<td>Degradation product HPLC</td>
<td>203.59-475.05 µmol L(^{-1}) (0.075-0.175 mg mL(^{-1}))</td>
<td>38 µmol L(^{-1}) (0.014 mg mL(^{-1}))</td>
<td>dosage forms (tablets and capsules)</td>
<td>100.35-101.21</td>
<td>(Förany, Haggag, Ragab, &amp; Elmallah, 2017)</td>
<td></td>
</tr>
<tr>
<td>chloroform and ethyl acetate extraction HPLC</td>
<td>0.013-0.067 µmol L(^{-1}) (5-25 ngmL(^{-1})) and 0.067-0.068 µmol L(^{-1}) (25-250 ngmL(^{-1}))</td>
<td>0.067 µmol L(^{-1})</td>
<td>plasma</td>
<td>66-78</td>
<td>(Pak, Patek, &amp; Mayersohn, 2003)</td>
<td></td>
</tr>
<tr>
<td>Extraction with ethyl acetate/methanol organic solvents HPLC</td>
<td>0.541-19 µmol L(^{-1}) (0.2-7.0 µg mL(^{-1}))</td>
<td>0.247 nmol L(^{-1}) (0.091 ng mL(^{-1}))</td>
<td>plasma and urine</td>
<td>&gt;96</td>
<td>(Heath, Pruitt, Brenner, &amp; Rock, 2003)</td>
<td></td>
</tr>
<tr>
<td>methanol precipitation LC-MS/MS</td>
<td>13.57-5429.17 nmol L(^{-1}) (5-2000 ng mL(^{-1}))</td>
<td>13.57 nmol L(^{-1}) (5 ng mL(^{-1}))</td>
<td>rat plasma</td>
<td>98-106</td>
<td>(W. Ma, Wang, Guo, &amp; Tu, 2015)</td>
<td></td>
</tr>
<tr>
<td>solid-phase extraction (SPE) cartridge based on the material of tributyl phosphate resin Capillary electrophoresis with amperometric detection (CE-AD)</td>
<td>3-700 µmol L(^{-1})</td>
<td>30 nmol L(^{-1})</td>
<td>extracts of turmeric</td>
<td>81.0-85.5</td>
<td>(Sun, Gao, Cao, Yang, &amp; Wang, 2002)</td>
<td></td>
</tr>
<tr>
<td>nickel chloride solution modified (NiCl(_2)) modified GCE Electrochemical (DPV)</td>
<td>10-600 µmol L(^{-1})</td>
<td>0.109 µmol L(^{-1})</td>
<td>human blood serum</td>
<td>99.9-100.3</td>
<td>(Zokhtareh &amp; Rahimnejad, 2018)</td>
<td></td>
</tr>
<tr>
<td>MIP-modified carbon paste electrode (MIP-CPE)</td>
<td>0.1-50 µmol L(^{-1})</td>
<td>10.1 nmol L(^{-1})</td>
<td>curcuma powder and cookies</td>
<td>90.77-105.7</td>
<td>(Q. Zhou, Zhou, Pan, &amp; Li, 2017)</td>
<td></td>
</tr>
<tr>
<td>GCE Electrochemical (CV)</td>
<td>9.9-107 µmol L(^{-1})</td>
<td>4.1 µmol L(^{-1})</td>
<td>spices</td>
<td>99-100</td>
<td>(Ziyatdinova, Nizamova, &amp; Budnikov, 2012)</td>
<td></td>
</tr>
<tr>
<td>AS(^{3+}) ions on palladium nanoparticles (PdNps)-coated graphite electrode (AS(^{3+})/PdNps/GE) Electrochemical (SWV)</td>
<td>0.03-0.6 µmol L(^{-1})</td>
<td>22 nmol L(^{-1})</td>
<td>marketed spices</td>
<td>–</td>
<td>(Çakır, Bücher, &amp; Arslan, 2015)</td>
<td></td>
</tr>
<tr>
<td>nitrogen and phosphorus dual-doped carbon dots (NP-Cdots) Fluorescence quenching</td>
<td>0.5-20 µmol L(^{-1})</td>
<td>58 nmol L(^{-1})</td>
<td>drinking water and the food samples</td>
<td>95.2-105.2</td>
<td>(Liu, Gong, Dong, Zhou, Shuang, &amp; Dong, 2018)</td>
<td></td>
</tr>
<tr>
<td>GCE/CaO(_2)O(_2)/N-CNTs/P-GO/CUR-imprinted poly (l-Cys) Electrochemical (DPV)</td>
<td>0.1-30 µmol L(^{-1})</td>
<td>30 nmol L(^{-1})</td>
<td>Serum</td>
<td>80-110.87</td>
<td>Present study</td>
<td></td>
</tr>
</tbody>
</table>
Table 3

<table>
<thead>
<tr>
<th>Sample Added (nmol L^-1)</th>
<th>Found (nmol L^-1)</th>
<th>Recovery (%)</th>
<th>RSD (%(n = 3))</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>600</td>
<td>614</td>
<td>102.33</td>
</tr>
<tr>
<td>2</td>
<td>800</td>
<td>887</td>
<td>110.87</td>
</tr>
<tr>
<td>3</td>
<td>1000</td>
<td>1060</td>
<td>106.00</td>
</tr>
<tr>
<td>4</td>
<td>2000</td>
<td>2010</td>
<td>100.20</td>
</tr>
<tr>
<td>5</td>
<td>5000</td>
<td>4000</td>
<td>80.00</td>
</tr>
<tr>
<td>6</td>
<td>7000</td>
<td>6730</td>
<td>96.14</td>
</tr>
<tr>
<td>7</td>
<td>10,000</td>
<td>9630</td>
<td>96.30</td>
</tr>
</tbody>
</table>

(K₄ 35 L mol^-1 (Nikitina, Zaryanov, Kochetkov, Karyakina, Yatsimirsky, & Karyakin, 2017)).

3.6. Real sample

In order to evaluation of the feasibility of proposed sensor, the serum sample spiked with various concentration of CUR and analyzed by DPV method. As shown in the Table 3 the recovery values are ranged from 80 to 110.87 % which confirmed the low interferences from the matrix can be happened for detection of CUR. Moreover, according to the data of Table 3, repeatability (RSD%) for triplicate detection of CUR in serum sample was in the range of 0.76–5.81 %. The real sample study obviously proved that introduced sensor is highly efficient and applicable for accurate and precise detection of CUR in different real samples such as biological samples.

4. Conclusion

Herein, an electrochemical sensor was designed through modification of GCE by CuCo₂O₄/N-CNTs/P-GO nanocomposite which followed by electrochemical covering the modified electrode surface by poly(-Cys) layer in presence of CUR. In the next step, removal of CUR from poly(-Cys) matrix created cavities with high affinity toward CUR according to the shape and functional groups. As far as we know it was the first time that aforementioned design was used for detection of CUR. The CV and EIS studies obviously demonstrated that catalytic and conductivity features potentially increased after dropping the CuCo₂O₄/N-CNTs/P-GO nanocomposite and formation of CUR-imprinted poly(-Cys) on the electrode surface. These phenomena were happened due to the synergic features such as catalytic activity of Cu-doping sites, high specific surface area of CNTs, electron-donor ability of P-doping sites, high conducting electrodes density at Fermi level of carbons of GO, and electron transfer facilitation of numerous specific cavities. The designed sensor was successfully used for detection of CUR in the wide linear ranges of 0.1–0.8 µmol L⁻¹ and 0.8–30 µmol L⁻¹, and acceptable LOD of 30 nmol L⁻¹. Moreover, the as-constructed electrochemical sensor was successfully used for detection of CUR in serum sample with favorable recoveries (80–110.87%). The obtained results proved that this simple and fast response method can be powerfully used for detection and monitoring of CUR in biological samples.

CRediT authorship contribution statement


Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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