

3D USCT at KIT

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University of Karlsruhe and Helmholtz Research Center Karlsruhe currently joined 8,500 employees, 20,000 students, 364 professors

Institute for Data Processing and Electronics





Ultrasound Computer Tomography



- Since > 30 years
- Basic idea: Surround object with ultrasound transducers in fixed setup
- Long term goal: Early breast cancer diagnosis
- Vision: diagnostics at Ø ≤ 5 mm? (Approx. 5% probability for metastases)



Breast imaging in fixed setup

3D USCT: Motivation and Basic Concepts

- Many USCT systems use:
 - Surrounding aperture:
 - 3 "modalities" are acquired in one step
 - Unfocussed data acquisition
 - "Post beam forming": Optimal focus in image reconstruction
 - Synthetic aperture focusing technique (SAFT)



Usually "hybrid approaches": 2D SAFT, focused in elevation on emission and reception



3D USCT: Challenges



Challenges	Solution strategies 3D USCT Generation I and II
Nyquist > 100 000 transducers	"Sparse Aperture" approach with 6 x 2 000 transducer positions (Accept artifacts and suppress)
Cheap, reproducible unfocussed transducers	In house designed transducers, automatic batch fabrication, dedicated channels, integrated amplification
3D aperture?	Feasible cylinder aperture and optimized semi-ellipsoidal aperture
Large amount of data at high data rates	Powerful DAQ Hardware and dedicated powerful DAQ Hardware
Demanding image reconstruction	Signal and image processing in Grid and in Hardware

Currently: "In-between Systems"





3D USCT I

- Cylindrical aperture
- 1920 transducers (12 000 pos.)
- 3.5 million A-Scans ~ 20 GB
- Proof of concept with static phantoms



- 3D USCT II
 - Optimized semi-ellipsoidal aperture
 - Rotation and translation
 - Powerful DAQ hardware: 6 s 2 min
 - Imaging of living tissue

Image Reconstruction at KIT



- 3D SAFT in spatial domain
 - Critical: Phase aberration correction f
 - Grating lobe suppression
 - Projection kernel optimized: ~200 MVoxel/s
- Transmission tomography
 - Speed of sound and attenuation volumes
 - 3D USCT I: FDK Algorithm (cone beam CT)
 - 3D USCT II: Geometry independent methods, ART or pseudo polar Fourier with compressive sampling

$$f(\vec{x}) = \sum_{(i,k)} T(A_{(i,k)}(\frac{\|\vec{x}_i - \vec{x}\| + \|\vec{x} - \vec{x}_k\|}{\hat{c}(\vec{x}_i, \vec{x}_k, \vec{x})}))$$

- f: image
- T: preprocessing
- A: A-scan
- c: speed of sound
- i: number of emitter
- k: number of receiver

SAFT Results with 3D USCT I





Current Status 3D USCT II





3D USCT II aperture and mechanics







Current Status USCT II





Conclusion



3D USCT I

- Feasible, if sparse aperture can be accepted
- Sub-millimeter resolution possible
- Acceptable contrast
- **3D USCT Generation II:**
 - Aperture optimization: Semi-ellipsoidal aperture
 - New DAQ: DAQ time ~ 2 min





Patient bed





Algorithms and Imaging N. V. Ruiter, M. Zapf, R. Dapp, T. Hopp, H. Gemmeke, et. al.

Grid Computing and HW Acceleration M. Hardt, R. Stotzka, M. Birk, M. Balzer, et. al.

Sensors G. Göbel, B. Kohout, et. al.

DAQ und Hardware D. Tsherniakhovski, S. Menshikov, et. al.

Design and Mechanics L. Berger, B. Osswald, T. Piller, W. Frank, et. al.

